#### Introduction

The frontal-parietal mirror circuit (FPMC) is active when individuals observe or perform a goal-directed behavior<sup>1</sup>. Evidence in macaques and humans suggest that the FPMC is extremely robust at the point when individuals code the goal of the motor act, enabling an observer to understand an agent's intentions<sup>2, 3</sup>. Recent theoretical hypotheses in the fields of computer science and machine learning suggest that data from the FPMC may have applications in robotics and artificial intelligence<sup>4</sup>. Recently, EEG data has been used to control brainmachine interfaces<sup>5, 6</sup>, move a cursor on a computer screen<sup>7</sup>, and access a smart phone  $app^8$ .

We used EEG to measure mu- and beta-ERD in left and right motor component clusters, while individuals observed and imitated an actor engaging in goal-directed actions where the outcomes were either ambiguous or unambiguous. We employed machine learning algorithms to classify single trial EEG data to determine if participants were observing an action vs. nonmovement controls, as well as discriminating between ambiguous or unambiguous goals. These results are discussed in the context of developing a hands-free, non-invasive neural devices that can assist senior citizens with mobility impairments in a Smart Home environment.

Task Design		
<section-header></section-header>		<image/>
Control		
Unambiguous		
Interval A "Setting" 0 - 2600 ms	Interval B "Grasp" 2800 - 5400 ms	Interval C "Goal" 5600 - 8200

*Figure 1.* Task. Participants were seated in front of a monitor with a large bowl of cereal to their left, a cup rack to their right, and a coffee mug directly in front of them. Participants observed and imitated the following stimuli: Top row) Ambiguous goal. Actor grasped a cup and used it to scoop cereal from the bowl to his left or placed the cup on a cup rack to his right. Middle) Non-action control. Actor performed no action for entire interval. Last row) Unambiguous goal. Actor grasped a cup and used it to drink. Each interval was preceded by a 2000 ms fixation cross (EEG baseline). Additionally, each interval was separated by a 200 ms fixation cross. A green fixation cross was presented after each trial for five seconds, during which the participants imitated the action. This was followed by a red fixation cross which cued the participants to complete the action and return to the "ready" position. This was followed by a blank screen presented at a jitter of 1500 to 3000 ms.

# Using EEG and Machine Learning to Predict Action Goals from Data in the Human Mirror System Lawrence P. Behmer Jr<sup>1</sup>, Jason Fairey<sup>2</sup>, Sabrina Gonzales<sup>1</sup>, Kenneth Albright<sup>1</sup>, Lisa R. Fournier<sup>1</sup>, and Larry Holder<sup>2</sup> <sup>1</sup>Visual Attention Lab; <sup>2</sup>School of Electrical Engineering and Computer Science





## Methods

### EEG Analyses:

- 32 Biosemi active electrodes sampled at 256 Hz
- Individual epochs (-2000 to 8200 ms) around onset each trial • Movement intervals were removed
- Trials with excessive noise (+/- 100 mv.) were removed prior to 1<sup>st</sup> ICA pass • Trials with noisy components (+/- 10 mv.) were removed prior to 2<sup>nd</sup> ICA pass • Right and left motor component clusters identified using DipFit2

- Within 15% residual variance
- Transformed data in frequency domain (4-60 Hz) in 2.25 sec intervals • Right and left clusters analyzed in mu (8-10 Hz) and beta-bands (16 - 22 Hz.)

# **Single Trial Classification**

- Components were run through a wavelet analysis, isolating the frequencies with the strongest signal to noise ratio for individual trials.
- Individual trials were normalized in reference to the pre-stimulus time period, then the period of time containing each video was averaged out. A set of "lag" features was also created using the difference between the different video intervals. Each feature was binned into 10 discrete values.
- determine how successful a Experiments were run to classification algorithm (Naïve bayes) could perform on a trial by basis. The class distribution was balanced using a trial randomized sub-sampling.
- As an additional experiment, the two action conditions (ambiguous and unambiguous) were combined into one "action" and then compared against the control. The results over several participants is shown on the right in figure 3. Accuracies of up to 80% were obtained.



**Participants**:

Design:

• 16 right-handed participants

12 blocks – 20 trials each block

cereal or hang mug)

from mug)

Participants observed and imitated:

• 96 ambiguous goal videos (scoop

• 48 non-action videos (no action)

96 unambiguous goal videos (drink











- control conditions
- Mu- and beta-ERD was stronger in interval B for ambiguous and unambiguous conditions versus controls and interval A.
- Mu-ERD was stronger for ambiguous vs. unambiguous actions during interval
- Additionally, naïve bayes classification yielded up to 80% accuracies when discriminating between action observation and non-movement controls. • Most importantly discrimination between all three conditions was slightly 25% above chance
- Previous work has suggested that the FPMC codes for the goal of the action, and not simply its transient components; however, increased activation may also be driven by task complexity<sup>9, 10</sup>
- Further experiments using the entire range of electrodes, components, and frequencies could alleviate the effect of inter-trial variability during machine learning.

# 529 - 535.

- 442, 164-171.

- Trans. 57(10), 2495-2505.
- Neuroimage.





#### Washington State University

data was able to successfully discriminate between ambiguous, unambiguous, and

The use of EEG in BMIs to discriminate between brain activity during action planning and observation is critical for the development of non-invasive devices that could be used to detect falls. In order to minimize errors, BMIs would need to be sensitive not just to movement, but a host of other cognitive processes associated with motor activity such as action perception.

## References

1. Rizzolatti, G., Sinigaglia, C., 2010. The functional role of the parieto-frontal mirror circuit: interpretations and misinterpretations. Nat. Rev. Neurosci. 11, 264 – 274. 2. Iacoboni, M., Molnar-Szakacs, I., Gallese, V., Buccino, G., Mazziotta, J.C., Rizzolatti, G., 2005. Grasping the intentions of others with one's own mirror neuron system. PLoS Biol. 3. 3. Fogassi, L., Ferrari, P.F., Gesierich, B., Rozzi, S., Chersi, F., Rizzolatti, G., 2005. Parietal lobe: From action organization to intention understanding. Science. 308, 662 - 667. 4. Metta, G., Sandini, G., Natale, L., Craighero, L., Fadiga, L., 2006. Understanding mirror neurons: A bio-robotic approach. Int Studies. 7(2), 197-232. 5. Hochberg, L.R., Serruya, M.D., Friehs, G.M., Mukand, J.A., Saleh, M., Caplan, A.H., et al., 2006. Neuronal ensemble control of prosthetic devices by a human with tetraplegia. Nature.

6. Hochberg, L.R., Bacher, D., Jarosiewicz, B., Masse, N.Y., Sineral, J.D., Vogel, J. 2012. Reach and grasp by people with tetraplegia using a neutrally controlled robotic arm. Nature. 485, 7. Li, Y., Long, J., Yu, T., Yu, A., Wang, C., Zhang, H., et al., 2010. An EEG-based BCI system for 2-D cursor control by combining mu/beta rhythm and P300 potential. Biomed Eng, IEEE 8. Campbell, A.T., Choudhury, T., Hu, S., Mukerjee, M.K., Rabbi, M., Raizada, R.D.S., 2012. Neuro-phone: Brain-mobile phone interface using a wireless EEG headset. MobiHeld 10 Proc second ACM SIGCOMM workshop on networking, systems, and applications on mobile handhelds. 3-8. 9. Behmer Jr., L.P., Fournier, L.R. Under review. Working memory affects the neural efficiency of the frontal-parietal mirror circuit during a novel action planning task: An EEG study. 10. Behmer Jr., L.P., Fournier, L.R. In preparation. The neural efficiency of action planning: Differences in ERD between high and low working memory groups